

## **APPENDIX VI**

### ***Quality Control in Radiation Therapy\****

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\* Taken from: American Association of Physicists in Medicine. Comprehensive QA for radiation oncology: Report of the AAPM Radiation Therapy Committee Task Group No. 40. *Med Phys* 1994;21(4):581-618.



**Table I**  
**QA of Cobalt-60 units**

Frequency	Procedure	Tolerance <sup>a</sup>
Daily	Safety	
	Door interlock	Functional
	Radiation room monitor	Functional
	Audiovisual monitor	Functional
	Mechanical	
	Lasers	2 mm
	Distance indicator (ODI)	2 mm
Weekly	Check of <i>source</i> positioning	3 mm
Monthly	Dosimetry	
	Output constancy	2%
	Mechanical checks	
	Light/radiation field coincidence	3 mm
	Field size indicator (collimator setting)	2 mm
	<b>Gantry</b> and collimator angle indicator	1 deg.
	Cross-hair centering	1 mm
	Latching of wedges, trays	Functional
	Safety interlocks	
	Emergency off	Functional
	Wedge interlocks	Functional
Annual	Dosimetry	
	Output constancy	2%
	Field size dependence of output constancy	2%
	Central axis dosimetry parameter constancy (PDD/TAR)	2%
	Transmission factor constancy for all standard accessories	2%
	Wedge transmission factor constancy	2%
	Timer linearity and error	1%
	Output constancy vs <b>gantry</b> angle	2%
	Beam uniformity vs <b>gantry</b> angle	3%
	Safety Interlocks	
	Follow test procedures of manufacturers	Functional
	Mechanical Checks	
	Collimator rotation isocenter	2 mm diameter
	<b>Gantry</b> rotation isocenter	2 mm diameter
	Couch rotation isocenter	2 mm diameter
	Coincidence of collimator, <b>gantry</b> , couch axis with isocenter	2 mm diameter
	Coincidence of radiation and mechanical isocenter	2 mm diameter
	Table top sag	2 mm
	Vertical travel of table	2 mm
	Field-light intensity	Functional

<sup>a</sup> The tolerance listed in the tables should be interpreted to mean that if a parameter either: (1) exceeds the tabulated value (e.g., the measured isocenter under **gantry** rotation exceeds 2 mm diameter); or (2) that the change in the parameter exceeds the nominal value (e.g., the output changes by more than 2%), then an action is required. The distinction is emphasized by the use of the term constancy for the latter case. Moreover, for constancy, percent values are  $\pm$  the deviation of the parameter with respect to its nominal value; distances are referenced to the isocenter or nominal SSD.

**Table II**  
**QA of Medical Accelerators**

Frequency	Procedure	Tolerance <sup>a</sup>
Daily	Dosimetry	
	<i>X-ray</i> output constancy	3%
	<i>Electron</i> output constancy <sup>b</sup>	3%
	Mechanical	
	Localizing lasers	2 mm
	Distance indicator (ODI)	2 mm
	Safety	
	Door interlock	Functional
	Audiovisual monitor	Functional
Monthly	Dosimetry	
	<i>X-ray</i> output constancy <sup>c</sup>	2%
	<i>Electron</i> output constancy <sup>c</sup>	2%
	Backup monitor constancy	2%
	<i>X-ray</i> central axis dosimetry parameter (PDD, TAR) constancy	2%
	<i>Electron</i> central axis dosimetry parameter constancy (PDD)	2 mm @ therapeutic depth
	<i>X-ray</i> beam flatness constancy	2%
	<i>Electron</i> beam flatness constancy	3%
	<i>X-ray</i> and <i>electron</i> symmetry	3%
	Safety Interlocks	
	Emergency off switches	Functional
	Wedge, <i>electron</i> cone interlocks	Functional
	Mechanical Checks	
	Light/radiation field coincidence	2 mm or 1% on a side <sup>d</sup>
	Gantry/collimator angle indicators	1 deg
	Wedge position	2 mm (or 2% change in transmission factor)
	Tray position	2 mm
	Applicator position	2 mm
	Field size indicators	2 mm
	Cross-hair centering	2 mm diameter
	Treatment couch position indicators	2 mm/1 deg
	Latching of wedges, blocking tray	Functional
	Jaw symmetry <sup>e</sup>	2 mm
	Field light intensity	Functional
Annual	Dosimetry	
	<i>X-ray/electron</i> output calibration constancy	2%
	Field size dependence of <i>x-ray</i> output constancy	2%
	Output factor constancy for <i>electron</i> applicators	2%
	Central axis parameter constancy (PDD, TAR)	2%
	Off-axis factor constancy	2%
	Transmission factor constancy for all treatment accessories	2%
	Wedge transmission factor constancy <sup>f</sup>	2%
	Monitor chamber linearity	1%
	<i>X-ray</i> output constancy vs <i>gantry</i> angle	2%
	<i>Electron</i> output constancy vs <i>gantry</i> angle	2%
	Off-axis factor constancy vs <i>gantry</i> angle	2%
	Arc mode	Mfrs. specs.

Frequency	Procedure	Tolerance <sup>a</sup>
Annual	Safety Interlocks	Functional
	Follow manufacturers test procedures	
	Mechanical Checks	2 mm diameter
	Collimator rotation isocenter	
	<i>Gantry</i> rotation isocenter	
	Couch rotation isocenter	
	Coincidence of collimator, <i>gantry</i> , couch axes with isocenter	
	Coincidence of radiation and mechanical isocenter	
	Table top sag	
	Vertical travel of table	2 mm

<sup>a</sup> The tolerances listed in the tables should be interpreted to mean that if a parameter either: (1) exceeds the tabulated value (e.g., the measured isocenter under *gantry* rotation exceeds 2 mm diameter); or (2) that the change in the parameter exceeds the nominal value (e.g., the output changes by more than 2%), then an action is required. The distinction is emphasized by the use of the term constancy for the latter case. Moreover, for constancy, percent values are  $\pm$  the deviation of the parameter with respect to its nominal value; distances are referenced to the isocenter or nominal SSD.

<sup>b</sup> All *electron* energies need not be checked daily, but all *electron* energies are to be checked at least twice weekly.

<sup>c</sup> A constancy check with a field instrument using temperature/pressure corrections

<sup>d</sup> Whichever is greater. Should also be checked after change in light field source.

<sup>e</sup> Jaw symmetry is defined as difference in distance of each jaw from the isocenter.

<sup>f</sup> Most wedges' transmission factors are field size and depth dependent.

**Table III**  
**QA of simulators**

Frequency	Procedure	Tolerance <sup>a</sup>
Daily	Localizing lasers	2 mm
	Distance indicator (ODI)	2 mm
Monthly	Field size indicator	2 mm
	<i>Gantry</i> /collimator angle indicators	1 deg
	Cross-hair centering	2 mm diameter
	Focal spot-axis indicator	2 mm
	Fluoroscopic image quality	Baseline
	Emergency/collision avoidance	Functional
	Light/radiation field coincidence	2 mm or 1%
	Film processor sensitometry	Baseline
Annual	Mechanical Checks	
	Collimator rotation isocenter	2 mm diameter
	<i>Gantry</i> rotation isocenter	2 mm diameter
	Couch rotation isocenter	2 mm diameter
	Coincidence of collimator, <i>gantry</i> , couch axes and isocenter	2 mm diameter
	Table top sag	2 mm
	Vertical travel of couch	2 mm
	Radiographic Checks	
	<i>Exposure</i> rate	Baseline
	Table top <i>exposure</i> with fluoroscopy	Baseline
	kVp and mAs calibration	Baseline
	High and low contrast resolution	Baseline

<sup>a</sup> The tolerances mean that the parameter exceeds the tabulated value (e.g., the measured isocenter under *gantry* rotation exceeds 2 mm diameter).

**Table IV**  
**QA of measurement equipment**

I, initial use for each mode used or following malfunction and repairs; E, each use (measurement sequence) or ongoing evaluation; B, each batch or box at appropriate energy (dosimeter element position should also be considered); D, documented and correction applied or noted in report of measurement; M, monthly.

Instrument type	Test	Frequency	Tolerance <sup>a</sup>
Local standard <sup>b</sup>	ADCL calibration	2y <sup>c</sup>	D
	Linearity	2y <sup>c</sup>	0.5%
	Venting	2y <sup>c</sup>	D
	Extra-cameral signal (stem effect)	I	0.5%
	Leakage	E	0.1%
	Redundancy check <sup>d</sup>	E	2%
	Recombination	I	D
	Collecting potential	E	D
Field instruments	Local std. comparison	2y	1%
	Linearity	2y	D
	Venting	2y	D
	Extra-cameral signal	2y	D
	Leakage	E	0.1%
	Recombination	I	D
	Collecting potential	E	D
Output check	Local std. comparison	M	1%
<i>Relative dose</i>			
TLD	Calibration	E	D
	Linearity	I	D
Film	<i>Dose</i> response	B	D
	Densitometer linearity	1y	D
	Processor uniformity/reproducibility	E	D
<i>Ion chamber</i>	Linearity	1y	D
	Extra-cameral signal	I	1%
Diodes	Energy dependence	I	D
	Extra-cameral signal	I	D
	Linearity	I	D
Positioning	Accuracy	E	2 mm
	Hysteresis	E	2 mm
Automated Scanners	Mechanical	I	2 mm
	Positional accuracy	E	1 mm
	Collecting potential of detector	E	D
	Detector linearity	I	0.5%
	Extra-cameral signal	I	0.5%
	Detector leakage	E	0.5%
	Accuracy of data analysis	I	1%
	Accuracy of printouts	I	1 mm

Instrument type	Test	Frequency	Tolerance <sup>a</sup>
Accessories	Thermometer Calibration	I	0.1 deg/C
	Barometer Calibration	3 mo	1 mm/Hg
	Linear rule Calibration	I	0.3%

<sup>a</sup> Percent values are  $\pm$  the deviation of the parameter with respect to the nominal, and distances are referred to the isocenter or nominal SSD.

<sup>b</sup> Local standard instrument has a calibration directly traceable to NIST and should be reserved for calibration of radiation beams, field instruments, and intercomparisons.

<sup>c</sup> Two years required by NRC. Without a redundancy program, this may be inadequate; with a redundancy program, dosimetry systems maintain calibration factors for significantly longer periods of time.

<sup>d</sup> With a *radionuclide* (e.g., Sr-90) or chamber intercomparison.

**Table V**  
**QA for treatment planning systems and monitor unit calculations**

Frequency	Test	Tolerance <sup>a</sup>
Commissioning and following software update	Understand algorithm	Functional
	Single field or <i>source</i> isodose distributions	2% <sup>a</sup> or 2 mm <sup>b</sup>
	MU calculations	2%
	Test cases	2% or 2 mm
	I/O system	1 mm
Daily	I/O devices	1 mm
Monthly	Checksum	No change
	Subset of reference QA test set (when checksums not available)	2% or 2 mm <sup>c</sup>
	I/O system	1 mm
Annual	MU calculations	2%
	Reference QA test set	2% or 2 mm <sup>d</sup>
	I/O system	1 mm

<sup>a</sup> % difference between calculation of the computer treatment planning system and measurement (or independent calculation).

<sup>b</sup> In the region of high *dose* gradients the distance between isodose lines is more appropriate than % difference. In addition, less accuracy may be obtained near the end of single *sources*.

<sup>c</sup> These limits refer to the comparison of *dose* calculations at commissioning to the same calculations subsequently.

<sup>d</sup> These limits refer to comparison of calculations with measurement in a water tank



**Table VI**  
**Treatment planning process**

Process	Related QA procedures
Positioning and immobilization	Port films. Laser alignment
Simulation	Simulator QA including image quality and mechanical integrity
Patient data acquisition (CT, MRI, manual contouring)	CT, MRI QA including image quality and mechanical integrity. Accuracy of mechanical contouring
Data transfer to treatment planning system	QA of the entire data transfer process, including digitizers, digital data transfer, etc.
Definitions of target volumes	Peer review, e.g., new patient planning conference, chart rounds
Aperture design	Independent check of delivery (e.g., port films), and peer review
Computation of dose distributions	Machine data from commissioning and QA of treatment machines. Accuracy and QA of treatment planning system
Plan evaluation	Peer review of plan, e.g., during chart rounds Independent check by radiation oncology physicist
Prescription	Written, signed, and dated
Computation of monitor units	Treatment planning system QA. Independent check within 48 h
Production of blocks, beam modifiers	QA for block cutting and compensator systems Port film review
Plan implementation	Review of set-up by treatment planning team. Chart review
Patient QA	Treatment plan review. Chart review after new or modified field, weekly chart review, port film review. <i>In vivo</i> dosimetry for unusual fields, critical organ doses (e.g., gonadal dose). Status check, follow up

**Table VII**  
**Factors affecting monitor unit (minute) calculations**

<b>Parameter</b>	<b>Related QA</b>
Patient surface contour	Periodic checks of caliper accuracy. Redundant patient measurements. Treatment planning system monthly QA
Collimator setting	Monthly simulator & treatment machine QA (Tables I-III)
Dose per monitor unit (minute) on the central axis as a function of collimator settings	Part of daily & monthly machine QA for a 10 x 10 cm field (Tables I and II) and annual recommissioning for output vs field size
Depth of the calculation (prescription) point	Periodic checks of caliper accuracy. Use of both lasers and ODI during patient setup to verify depth. Repeat patient measurements during course of treatment
Target-to-patient-surface or target-to-isocenter distance	Monthly QA on simulators and treatment machines (Tables I-III)
Relative dose factors (PDD, TPR, TMR, etc.)	Monthly x-ray and electron energy constancy checks (Table II)
Aperture size and shape	Redundant check of magnification factor
Wedge and compensator transmission	Annual machine recommissioning. Monthly check of latches and positioning of accessories (Table II)
Blocking tray transmission	Annual machine recommissioning. Monthly check of latches and positioning of accessories (Table II)

**Table VIII**  
**Summary of QA recommendations for individual patients**

Procedure	Recommendation
Monitor unit (minutes) calculations	1. Reviewed prior to treatment by an authorized individual who did not perform initial calculation, or when not possible (e.g., emergency treatment), then prior to 3rd fraction or before 10% of the <i>dose</i> has been delivered, whichever occurs first.
Graphical treatment plan review	<ol style="list-style-type: none"> <li>1. Reviewed prior to treatment, or when not possible, then prior to 3rd fraction or before 10% of the <i>dose</i> has been delivered, whichever occurs first.</li> <li>2. Reviewed by a radiation oncology physicist who did not formulate treatment plan. Where only one physicist and that person performed the plan, then reviewed by another authorized individual.</li> <li>3. Review includes calculated monitor units, input-output and plan quality.</li> <li>4. Independent calculation of <i>dose</i> at a point: Compare for each field—with an independent calculation of <i>dose</i> to a point using the calculated monitor units—the prescribed and calculated <i>dose</i>.</li> <li>5. If these differ by more than 5%, then the discrepancy should be resolved before continuing treatment.</li> </ol>
Plan set-up	Radiation oncologist present at first setup or for major changes in treatment.
Beam (portal) films—curative and high morbidity risk palliative patients	Initial films reviewed by radiation oncologist prior to first treatment. In addition, ongoing portal films (the standard is weekly) also reviewed by the radiation oncologist
Beam (portal) films—palliative patients	Films reviewed prior to second fraction.
<i>In-vivo</i> dosimetry	<ol style="list-style-type: none"> <li>1. All institutions should have access to TLD or other <i>in vivo</i> dosimetry systems.</li> <li>2. Should be used to measure <i>dose</i> to critical structures (e.g., lens, gonads).</li> <li>3. May be used to record <i>dose</i> for unusual treatment conditions.</li> </ol>

**Table IX**  
**QA tests for brachytherapy sources**

I, initial purchase; D, documented, and E, at every use

Type of Source	Test	Frequency	Tolerance
Long <i>half-life</i> : description	Physical/chemical form	I	D
	Source encapsulation	I	D
	Radionuclide distribution and uniformity	I	D
	Location of radionuclide	I	1 mm
Long <i>half-life</i> : calibration	Mean of batch	I	3%
	Deviation from mean	I	5%, D
	Calibration verification	E	
Short <i>half-life</i> : description	Physical/chemical form	I	D
	Source encapsulation	I	D
Short <i>half-life</i> : calibration	Mean of batch	E	3%
	Deviation from mean <sup>b</sup>	E	5%
	Radionuclide distribution and source uniformity	E	V <sup>c</sup>

<sup>a</sup> Visual check of source color code or measurement in a *calibrator*.

<sup>b</sup> For short *half-life* sources this may not always be practical.

<sup>c</sup> V, visual check, autoradiograph, or ionometric check.

**Table X**  
**QA tests for brachytherapy source calibrator**

I, initial use or following malfunction and repairs, S, *isotope/source* specific, D, documented and correction applied or noted in report of measurement, when appropriate, and E, each use (measurement sequence) or ongoing evaluation.

Instrument Type	Test	Frequency	Tolerance
Well ionization chamber	ADCL calibration	I,S <sup>a</sup>	D
	Precision	I	2%
	Linearity	I, 2 year	1%
	Collection Efficiency	I	1%
	Geometrical/length dependence	I	D
	Energy dependence	I	D
	Wall dependence	I	D
	Venting	I	D
	Redundant check	E	2%
	Leakage	E	D
In-air calibration chamber and external holder	ADCL calibration	I,S <sup>a</sup>	D
	Accuracy of chamber distance	1 yr, S	1%, D
	Redundancy	E	D
	See Table IV for other tests		

<sup>a</sup> Instrument or source have a calibration directly traceable to NIST.

**Table XI**  
**QA tests for brachytherapy applicators**

I, initial use or following malfunction and repairs; D, documented and correction applied or noted in report of measurements, when appropriate; and E, as a minimum, a visual inspection to verify that the dummy source fairly represent the active *source* distribution.

Type of applicator	Test	Frequency	Tolerance
Intracavitary	Location	I <sup>a</sup> , yearly	D
	Coincidence of dummy and active <i>sources</i>	I	1 mm
	Location of shields	I <sup>b</sup>	D
Interstitial	Coincidence of dummy and active <i>sources</i>	I,E	1 mm

<sup>a</sup> To reduce personnel *exposure*, the dummy *source* location may be checked in place of the active, if it is established that the dummy and active *source* locations are coincident.

<sup>b</sup> Location of shields should be verified by radiograph before the first use. Before every use, the applicator may be shaken to listen for loose parts.

**Table XII**  
**Procedure specific parameter verification**

Endpoint	Procedure	When
Accuracy of OR implant description	Direct observation	During procedure
Prescription accuracy and consistency	Consistency of loading and prescription with disease stage, therapy chart treatment plan, department treatment policies	First half of treatment
Verify correct <i>source</i> chosen	Spot calibration check and visual verification	preparation and <i>source</i> loading
<i>Sources</i> correctly loaded	Therapist or physicist (or individual knowledgeable in <i>source</i> loading) always assists physician	loading
Treatment plan	Calculation of plan and check for accuracy/consistency	First half of treatment
Implant removal	Physicist present or contact nursing staff to verify	Expected removal time
<i>Sources</i> all removed	Patient survey <i>source</i> count Final <i>source</i> inventory	At removal Next working day
Review treatment	Verify treatment time	After completion of procedure
Record, QA audit	All QA, treatment, and radiation safety records complete	After completion of procedure

**Table XIII**  
**QA of remote afterloading brachytherapy units**

Frequency	Test	Tolerance
Each treatment day	Room safety door interlocks, lights, and alarms	Functional
	Console functions, switches, batteries, printer	Functional
	Visual inspection of <i>source</i> guides	Free of kinks and firmly attached
	Verify accuracy of ribbon preparation	Autoradiograph
Weekly	Accuracy of <i>source</i> and dummy loading (dummies used for spacing and/or simulation/verification)	1 mm
	<i>Source</i> positioning	1 mm
At each <i>source</i> change or quarterly	Calibration <sup>a</sup>	3%
	Timer function	1%
	Check accuracy of <i>source</i> guides and connectors	1 mm
	Mechanical integrity of applicators (by <i>x ray</i> if appropriate)	Functional
Annual	<i>Dose</i> calculation algorithm (at least one standard <i>source</i> configuration for each <i>isotope</i> ). Simulate emergency conditions. Verify <i>source</i> inventory	3%, 1 mm

<sup>a</sup> It is worthwhile at *source* change to calibrate both new and old *sources* to establish and document reproducibility of calibration method.

## **APPENDIX VII**

### **Standards of the American College of Radiology\***

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\* Taken from: American College of Radiology. *Standards*. Reston: ACR; 1997.





**Diagnostic Radiology**

1. ACR Standard for General (Plain) Radiography
2. ACR Standard for Communication-Diagnostic Radiology
3. ACR Standard for Teleradiology
4. ACR Standard for Diagnostic Medical Physics Performance Monitoring of Radiologic and Fluoroscopic Equipment
5. ACR Standard for the Performance of Computed Tomography in the Evaluation of Head Trauma
6. ACR Standard for Skeletal Surveys in Children
7. ACR Standard for the Performance of Pediatric and Adult Chest Radiography
8. ACR Standard for the Performance of Pediatric and Adult Bedside Chest Radiography (Portable Chest Radiography)
9. ACR Standard for the Performance of Thoracic Computed Tomography
10. ACR Standard for the Performance of Computed Tomography of the Abdomen and Pelvis
11. ACR Standards for the Performance of Screening Mammography
12. ACR Standard for the Performance of Diagnostic Mammography and Problem-Solving Breast Evaluation
13. ACR Standard for the Performance of Adult Esophagrams and Upper Gastrointestinal Examinations
14. ACR Standard for the Performance of Per Oral Barium Small Bowel Examinations in Adults
15. ACR Standard for the Performance of Adult Enteroclysis Examinations
16. ACR Standard for Performance of Adult Barium Enema Examinations
17. ACR Standard for the Performance of Pediatric Contrast Examinations of the Upper Gastrointestinal Tract
18. ACR Standard for the Performance of Pediatric Contrast Enema Examinations
19. ACR Standard for the Performance of Excretory Urography
20. ACR Standard for the Performance of Adult Cystography and Urethrography
21. ACR Standard for the Performance of Voiding Cysturethrography in Children
22. ACR Standard for the Performance of Magnetic Resonance Imaging

**Interventional Radiology**

1. ACR Standard for the Use of Intravenous Conscious Sedation
2. ACR Standard for the Performance of Cerebral Angiography
3. ACR Standard for the Performance of Myelography
4. ACR Standards for Diagnostic Arteriography in Adults
5. ACR Standard for the Performance of Stereotactically-Guided Breast Interventional Procedures
6. ACR Standard for the Performance of Ultrasound-Guided Percutaneous Breast Interventional Procedures

7. ACR Standard for the Performance of Imaging-Guided Trans-Thoracic Needle Biopsy in Adults
8. ACR Standard for the Performance of Imaging-Guided Percutaneous Thoracic Aspiration or Catheter Drainage in Adults
9. ACR Standard for the Performance of Percutaneous Nephrostomy

#### **Nuclear Medicine**

1. ACR Standard for Imaging for Radiopharmaceuticals
2. ACR Standard for the Performance of Cerebral Scintigraphy for Brain Death
3. ACR Standard for the Performance of Skeletal Scintigraphy
4. ACR Standard for the Performance of Cardiac Scintigraphy
5. ACR Standard for the Performance of Thyroid Scintigraphy and Uptake Measurements
6. ACR Standard for the Performance of Parathyroid Scintigraphy
7. ACR Standard for the Performance of Pulmonary Scintigraphy
8. ACR Standard for the Performance of Gastrointestinal Scintigraphy
9. ACR Standard for the Performance of Hepatobiliary Scintigraphy
10. ACR Standard for the Performance of Liver/Spleen Scintigraphy
11. ACR Standard for the Performance of Renal Scintigraphy
12. ACR Standard for the Performance of Radionuclide Cystography
13. ACR Standard for the Performance of Scrotal Scintigraphy
14. ACR Standard for the Performance of Infectious and Inflammatory Conditions
15. ACR Standard for the Performance of Tumor Scintigraphy
16. ACR Standard for the Performance of Therapy with Unsealed *Radionuclide* Sources

#### **Radiation Oncology**

1. ACR Standard for Radiation Oncology
2. ACR Standard for the Performance of Radiation Oncology Physics for External Beam Therapy
3. ACR Standard for the Performance of High-Dose-Rate Brachytherapy
4. ACR Standard for the Performance of Low-Dose-Rate Brachytherapy
5. ACR Standard for the Performance of Brachytherapy Physics: Manually-Loaded Sources
6. ACR Standard for 3D External Beam Radiation Planning and Conformal Therapy
7. ACR Standard for the Performance of Stereotactic Radiation Therapy/Radiosurgery
8. Standard for Diagnosis and Management for Invasive Breast Carcinoma
9. Standards for Diagnosis and Management of Ductal Carcinoma In-Situ of the Breast (DCIS)
10. ACR Standard for the Performance of Therapy with Unsealed Radionuclide Sources

**Ultrasound**

1. ACR Standard for Performing and Interpreting Diagnostic Ultrasound Examinations
2. ACR Standard for the Performance of an Ultrasound Examination of the Extracranial Cerebrovascular System
3. ACR Standard for Performance of the Pediatric Neurosonology Examination
4. ACR Standard for the Performance of Peripheral Arterial Ultrasound Examination
5. ACR Standard for Performance of the Peripheral Venous Ultrasound Examination
6. ACR Standard for the Performance of the Thyroid and Parathyroid Ultrasound Examination
7. ACR Standard for the Performance of Breast Ultrasound Examination
8. ACR Standard for the Performance of Abdominal, Renal, or Retroperitoneal Ultrasound Examination in Infants, Children, and Adults
9. ACR Standard for the Performance of Ultrasound Examination of the Female Pelvis
10. ACR Standard for the Performance of Antepartum Obstetrical Ultrasound
11. ACR Standard for the Performance of Ultrasound Evaluation of the Prostate (and surrounding structures)
12. ACR Standard for the Performance of Scrotal Ultrasound Examination

**Credentialing**

1. ACR Standard for Continuing Medical Education (CME)

**Magnetic Resonance Imaging****MRI Monograph**



## **APPENDIX VIII**

### **Radiation Protection Data**



## Appendix VIII-A

***Values of the Radiation Weighting Factor ( $W_R$ )***

***and the Tissue Weighting Factor ( $W_T$ )\****

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\* Taken from: Food and Agriculture Organization of the United Nations, International Atomic Energy Agency, International Labour Organisation, Nuclear Agency of the Organisation for Economic Co-operation and Development, Pan American Health Organization, World Health Organization. *International basic safety standards for protection against ionizing radiation and for the safety of radiation sources*. Vienna: International Atomic Energy Agency; 1997. (Safety series 115).





**Values of the Radiation Weighting Factor ( $W_R$ )  
and the Tissue Weighting Factor ( $W_T$ )**

Type and energy range of radiation	Radiation weighting factor, $W_R$
<i>Photons</i>	1
<i>Electrons</i>	1
<i>Neutrons</i>	
< 10 keV	5
100 keV to 2 MeV	20
2 MeV to 20 MeV	10
> 20 MeV	5
<i>Protons</i> > 2 MeV	5
<i>Alpha particles</i>	20

Tissues or organs	Tissue weighting factor, $W_T$
Bone surfaces - skin	0.01
Liver - breast - bladder - oesophagus - thyroid - remainder	0.05
Bone marrow (red) - colon - lung - stomach	0.12
Gonads	0.20



## **Appendix VIII-B**

### ***Sources of Exposure to Ionizing Radiation\****

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\* Taken from: United Nations Scientific Committee on the Effects of Atomic Radiation. *Sources and effects of ionizing radiation*. New York: UN; 1993. (UNSCEAR 1993 Report to the General Assembly).



### *Sources of Exposure to Ionizing Radiation*

<i>Natural Sources</i>	<i>Average Annual Effective Dose (mSv)</i>
<i>Cosmic rays</i>	0.39
<i>Terrestrial gamma rays</i>	0.46
<i>Radioisotopes in the body (except radon)</i>	0.23
<i>Radon and its decay products</i>	1.3
<i>Total</i>	2.4

<i>Artificial Sources</i>	<i>Average Annual Effective Dose (mSv)</i>
Medical <i>sources</i>	0.6
Nuclear explosions	0.01
Nuclear energy	0.0002

<i>Sources for Medical Use</i>	<i>Number</i>
<i>X-ray</i> units (diagnosis)	720,000
<i>X-ray</i> units (therapy)	13,000
Cobalt therapy and caesium units	4,000
<i>Accelerators</i>	1,800
Nuclear medicine clinics	13,000
"Spent" Radioactive <i>sources</i> (in disuse)	130,000

Annual *collective dose* due to diagnostic radiology: 1,600,000 man Sv



## **Appendix VIII-C**

### ***Threshold Dose Values for Deterministic Effects\****

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\* Taken from: International Commission on Radiological Protection. 1990 Recommendations of the International Commission on Radiological Protection. ICRP Publication 60. *Ann ICRP* 1991 21(1-3).





**Threshold Dose Values for Deterministic Effects**

<i>Deterministic Effect</i>	<i>Dose Equivalent Threshold (Single Exposure) (Gy)</i>
Permanent Sterility	
Males	3.5 - 6.0
Females	2.5 - 6.0
Lens Opacity	0.5 - 2.0
Cataracts	5.0
Hematopoietic Depression	0.5



## Appendix VIII-D

### *Dose Limits\**

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\* Taken from: Food and Agriculture Organization of the United Nations, International Atomic Energy Agency, International Labour Organisation, Nuclear Agency of the Organisation for Economic Co-operation and Development, Pan American Health Organization, World Health Organization. *International basic safety standards for protection against ionizing radiation and for the safety of radiation sources*. Vienna: International Atomic Energy Agency; 1997. (Safety series 115).



## *Dose Limits*

The annual *effective dose limit* for *workers* in accordance with the *BSS* (26) is 20 mSv per year (not to exceed 50 mSv per year averaged over 5 consecutive years), and the annual *equivalent dose* to the extremities (hands and feet) or the skin is 500 mSv and to the lens of the eye, 150 mSv. For *members of the public*, the annual *effective dose limit* has been established at 1 mSv; the *equivalent dose* to the extremities is not to exceed 50 mSv, and to the lens, 15 mSv.

In monitoring compliance with these *limits*, both *doses*, those generated by external *sources* and the committed *doses* from *radionuclide* intakes into the body, must be taken into account. However, *doses* from natural radiation and those incurred by people as patients undergoing medical procedures with radiation *sources* should not be included.

In the case of pregnant female *workers*, once pregnancy is declared and during the rest of gestation, the *equivalent dose* to the embryo/fetus should not exceed 1 mSv.

For students between 16 and 18 years of age, the recommended annual *limits* are as follows: *Effective dose*, 6 mSv; *equivalent dose* to the lens, 50 mSv, and to the skin or the extremities, 150 mSv.

